

## Performance evaluation of Cryo Laser Phoresis technique as biophysical method to promote diclofenac sodium cutaneous perfusion

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Aiming to alter and/or improve permeation of active compounds in the skin, many strategies have been developed, including biophysical methods. One of the physical absorption techniques, currently known as Cryo Laser Phoresis (CLP), consists of an apparatus that emits radiation on polar or nonpolar molecules of the active substance, resulting in faster penetration when in comparison to the standard topical application. The goal of this work was to evaluate the efficacy of a method that proposes to increase cutaneous permeation of diclofenac sodium by using CLP technique. The influence on permeation was evaluated *ex vivo*, using Franz cell and human skin obtained from cosmetic surgery. The results were evaluated using statistical methods and data exploratory analysis: clusters, k-means and Principal Component Analysis. The results showed a larger increase in the concentration of diclofenac sodium in the dermis with the use of laser. In all samples (with or without laser application) it was observed that skin surface showed an amount of diclofenac sodium and that there was no active passage to the receptor liquid, suggesting that diclofenac sodium was not absorbed. These results indicate that CLP, when used under the conditions described in this study, is able to increase diclofenac sodium penetration and its retention into deeper layers.

**Uniterms:** Cryo Laser Phoresis/dematologic use. Cutaneous permeation. Diclofenac sodium/cutaneous permeation. Franz cell.

No sentido de alterar e/ou melhorar a penetração de substâncias na pele, diversas estratégias têm sido desenvolvidas, variando desde a aplicação de novos veículos e ativos encapsulados, até equipamentos que atuam por métodos biofísicos. Uma das técnicas de absorção física, atualmente conhecida como Crio Laser Forese (CLF), consiste em um aparato que emite radiação sobre moléculas polares ou apolares da substância ativa, tornando sua penetração mais rápida, se comparada à administração tópica comum. O objetivo deste trabalho foi avaliar a eficácia de um método que propõe aumentar a permeação cutânea do diclofenaco de sódio incorporado a um gel, por meio do uso da CLF. A influência sobre a permeação foi avaliada *ex vivo*, utilizando célula de Franz e pele humana obtida de cirurgia plástica. Os resultados foram balizados mediante aplicação de métodos estatísticos e análise exploratória de dados: clusters, k-means e Análise por Componentes Principais. Os resultados demonstraram aumento na concentração do diclofenaco de sódio na derme com o uso do laser. Em todas as amostras (com ou sem aplicação de laser), observou-se, uma quantidade de diclofenaco de sódio na superfície da pele e que não houve passagem de ativo para o líquido do receptor, sugerindo que o diclofenaco de sódio não foi absorvido. Estes resultados indicam que CLF usada sob as condições descritas neste estudo é capaz de aumentar a penetração do diclofenaco de sódio e sua retenção em camadas mais profundas da pele

**Unitermos:** Crio Laser Forese/uso em dermatologia. Permeação cutânea. Diclofenaco de sódio/permeação cutânea. Célula de Franz.

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## INTRODUCTION

The skin has many functions and amongst them it is possible to emphasize its role as a barrier against exogenous agents, its utility to keep the homeostasis of the organism and to prevent internal water loss. Beyond that, it has been shown that it is an appropriate route for treatment systems, through transdermal administration of drugs (Leite-Silva *et al.*, 2012). Several methods have been developed to increase the penetration of substances through skin. This includes the use of substances that act as permeation enhancers (chemical enhancers) in formulations or the development of new methods that modify the lipid and protein organization, inter and intracellular of the stratum corneum (biophysical enhancers) and can reversibly decrease the skin's barrier property (Lopes *et al.*, 2008; Silva *et al.*, 2010).

Throughout the years there was a significant growth of knowledge in biochemical and metabolic processes involving substance flow through skin (Fluhr, Feingold, Elias, 2006). There are many factors that influence substance permeation through skin, such as formulation, particle size, component concentration, skin thickness, pH and sebum production, among others (Gallagher *et al.*, 2003; Benson, 2005; Trommer, Neubert, 2006; Baroli, 2010; Leite-Silva *et al.*, 2012).

Several methods have been formulated to promote augmentation of transdermic transportation, having obtained varying levels of success. The promoting agents of chemical absorption can improve the skin's permeability to small molecules, but also can lead to irritation of the surface of the skin or other factors that may limit their use. Iontophoresis uses electric fields to permeate ionized molecules through the skin using electrophoresis and electroosmosis for non-ionized molecules. This technique can be useful for applications that contain peptides and small proteins. Physical methods that temporarily improve skin permeability such as electroporation and ultrasound are used, representing perspectives in the application of drugs of low or high molecular weight (Patil, Saraogi, 2014). However, not much studying has been done about the use of CryoLaser as a method of biophysical permeation.

In spite of the use of chemical permeation enhancers being widely studied, remarkable attention has been given to the benefits of biophysical permeation promoting techniques. One of them is known as Cryo Laser Phoresis (CLP), also named Cryopass Therapy, developed by C.I.R.C.E srl – Italy (Bonizzoni, 2007). It is applied with a device called Lasericemed, which emits a laser radiation on polar or nonpolar active substances and claims to make

their absorption faster and more efficient when compared to the standard topical administration. The laser emission releases photons that collide with electrons of active substance molecules. This impact leads to photon energy transfer to electrons from more external orbitals, as kinetic energy form. This increases gravitational acceleration, allowing molecules to pass through skin and be delivered to the desired site (Terraneo *et al.*, 2011).

The aim of this work was to evaluate the Cryo Laser Phoresis efficiency as biophysical method to promote diclofenac sodium cutaneous permeation.

## MATERIAL AND METHODS

### Material

Hydroxyethylcellulose (CAS 9004-62-0, Mapric Produtos Farmacosmeticos). The diclofenac sodium working standard (monosodium acid 2-[(2,6-dichlorophenyl) amino] benzene acetic salt) was donated by Medley Pharmaceutical Industry and methylchloroisothiazolinone and methylisothiazolinone were donated by Pro-ServQuimica LTDA. Acetonitrile (J. T. Baxter™) and methanol (J. T. Baxter™) were from HPLC grade and phosphate buffer (PBS) components (NaCl - MW: 58,44; KCl - MW: 74,55; Na<sub>2</sub>HPO<sub>4</sub> - MW: 141,96 and KH<sub>2</sub>PO<sub>4</sub> - MW: 136,09) were P. A. grade from Synth®. The *tape stripping* tapes (Standard S-Squame Disc CuDe 15109) were from CuDerm. The syringe filters Millex were from Milipore®. The C18 chromatography column within 25 cm x 4.6 mm dimensions, 5 µm particle size was from ACE™.

### Formulation

A gel was formulated using low irritant power and low cost raw materials (Table I). The gel was frozen until -20 °C in suitable a package to attach to the device.

### Permeation test

UNIFESP's Ethics Committee previously approved the use of skin obtained by excision in cosmetic surgery, with protocol number 631972. After preparation, the skin was stored at a temperature of approximately -20 °C.

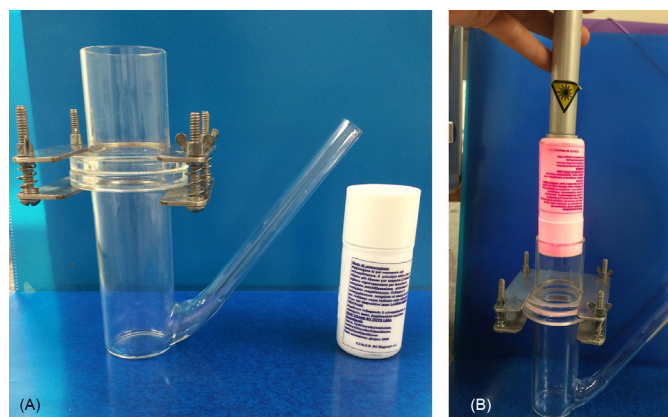
The experiment was performed using dual compartment vertical diffusion cells (Franz cells) that were specifically modified and adapted exclusively for this experiment, with the superior portion suitable to receive a package that will be connected to the laser (Figure 1A). The skin was rehydrated for one hour with

**TABLE I** - Composition of formulations (% w/w) evaluated

Ingredient	F1	F2	F3
Hydroxyethylcellulose	0.6	0.6	0.6
Methylchloroisothiazolinone (and) Methylisothiazolinone	0.1	0.1	0.1
Diclofenac Sodium	1.0	1.5	2.0
Water	98.3	97.8	97.3

phosphate buffer (PBS) pH 7.4. PBS was added to the receptor compartment and the system was immersed in a bath at 37 °C, and stirred continuously for half an hour to stabilize the system.

The bottle containing the active frozen gel was attached to the device and placed in contact with the skin for 10 min, with or without laser contact, in this case, employing the device Lasericemed turned on (Figure 1B). It is just an illustration, without the human skin and the receptor liquid only to demonstrate how the laser is used. This study was performed in triplicate.



**FIGURE 1** - (A) Adapted Franz cell and the package where the gel was frozen; (B) Simulation of the laser attached to the package that contains diclofenac sodium frozen gel.

The receptor liquid was collected at intervals of 10 and 20 min. After 20 min, the gel applied to skin surface was removed with swabs™. Next, stratum corneum (SC) extraction was performed by “tape stripping” technique and the detachment of epidermis from dermis was performed (water at 60 °C for 90 s). The samples were stored after being soaked in methanol for approximately 15 min.

Afterwards, an aliquot from the supernatant liquid from each sample was removed and submitted to HPLC analysis. The final samples were: 10 min receptor liquid, 20 min receptor liquid, swab, tapes 1-5, tapes 6-10, epidermis and dermis, with and without laser application.

### Determination of diclofenac sodium in the samples

The methodology of diclofenac sodium analysis was developed based on conditions described on USP 35 (2013) monograph and also on the methodology described by Klimes *et al.* (2001).

Considering these aspects, the chromatographic quantification of diclofenac sodium was performed by using HPLC degree solvents (acetonitrile and methanol) and C18 chromatography column within 25 cm x 4.6 mm dimensions, 5 µm particle size. Diclofenac sodium (working standard), with 99% purity was used as secondary standard. The analyses were performed in a liquid chromatograph model ACELLA 600, from Thermo Scientific™, equipped with quaternary pump system, column oven, automatic injector and diode array detector (DAD). Data was processed by ChromQuest™ software.

In addition, the following chromatography system parameters were also evaluated: retention factor, asymmetry (10%) and number of theoretical plates, according to (USP 35, 2013) recommended parameters.

In connection with the sample preparation, with 0.5 mL fixed volume, all samples were previously filtered through 0.45 µm syringe filters and stored in 1.5 mL vials. The samples were diluted, when necessary, so active expected concentrations were coherent with the ones determined at calibration curve. Chromatography conditions for diclofenac sodium analysis were based on the US Pharmacopoeia (USP 35), with some modifications for optimizing the method, according to gel matrix and biological matrix content, assessing parameters as: stationary phase and chromatographic column dimensions, content, mobile phase flow, temperature, injection volume, sample solution and standard solution concentration related to HPLC equipment response.

After optimization, an isocratic method was established with mobile phase composed of 30% phosphate buffer (pH 2.5) and 70% acetonitrile, with 1.0 mL.min<sup>-1</sup> flow, using C18 column with 25 cm x 4.6 mm, 5 µm particle size and DAD detector monitoring 254 nm

wavelength. The injected volume of each sample was 25  $\mu\text{L}$  and 9 min run time.

A stock solution was prepared in a volumetric flask, transferring 12.5 mg of diclofenac sodium in 25 mL of methanol, obtaining a 500  $\mu\text{g}\cdot\text{mL}^{-1}$  solution. From the stock solution and using 10 mL volumetric flasks, dilutions were prepared leading to the concentrations: 2.5; 5.0; 12.5; 25; 50; 100 and 150  $\mu\text{g}\cdot\text{mL}^{-1}$  in methanol. The standard concentrations for the calibration curve were prepared in triplicate and analyzed in the previously described chromatography conditions.

### Statistical analysis

At the data exploratory phase, *t Student* test was applied, which allowed verifying significant differences between “With Laser” and “Without Laser” situations, to the Dermis (D). Given the hypothesis absence, a priori, to all other results, *cluster* analysis method application was chosen ( $p$ -value < 0.05 was considered to be statistically significant).

## RESULTS AND DISCUSSION

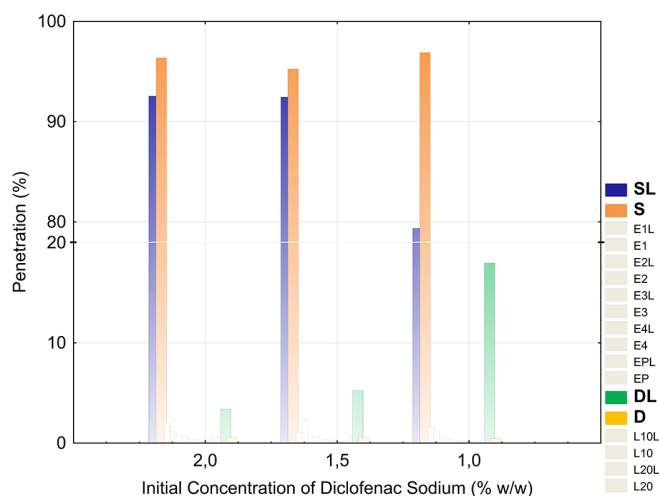
Diclofenac sodium was chosen as a marker due to its hydrophilic characteristics that hinder its flow through the skin’s lipid layer (Lopes *et al.*, 2008) and because it can be a good alternative for challenging the biophysical enhancer. Gaur *et al.* (2014) had studied the transdermal formulations containing permeation enhancers that cause skin damage and diclofenac was used as a model drug. The presence of ceramid specifically promotes drug permeation through SC and dermis and also contributes to stability and non-irritancy.

Escribano *et al.* (2003) evaluated the transdermal permeation of sodium diclofenac. Permeation studies were carried out *in vitro* using human skin from plastic surgery as a membrane – as we did in our research. However, they used chemical enhancers instead of biophysical methods to improved diclofenac permeation.

The influence of an erbium:YAG laser on the transdermal delivery of drugs across skin was studied *in vitro* by Lee *et al.* (2001). The researchers concluded that the use of an erbium:YAG laser is a good method for enhancing transdermal absorption of both lipophilic and hydrophilic drugs, because it allows precise control of SC removal, and this ablation of SC can be reversible to its original normal status. Nevertheless, the laser used in this work does not have ablation potential.

The Figure 2 shows the comparative performance of samples submitted to the laser treatment and not submitted

to the laser treatment; highlighted are the Swab and dermis samples, in gray are the other samples with inexpressive graphic representation.

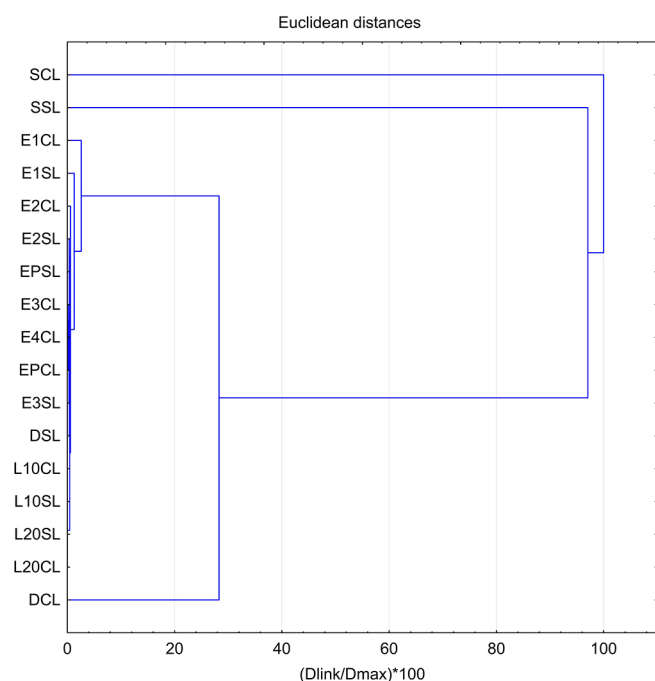


**FIGURE 2** - Comparative performance of samples submitted to the laser treatment and not submitted to laser treatment. Notes: SL = Swab with laser; S = Swab without laser; E1L = tape strip 1 to 5 with laser; E1 = tape strip 1 to 5 without laser; E2L = tape strip 6 to 10 with laser; E2 = tape strip 6 to 10 without laser; E3L = tape strip 11 to 15 with laser; E3 = tape strip 11 to 15 without laser; E4L = tape strip 16 to 20 with laser; E4 = tape strip 16 to 20 without laser; EPL= epidermis with laser; EP= epidermis without laser; DL= Dermis with laser; D= Dermis without laser; L10L= receptor liquid 10 min with laser; L10= receptor liquid 10 min without laser; L20L= receptor liquid 20 min with laser; L20= receptor liquid 20 min without laser.

The statistical analysis reinforces the validity of these data. The Figure 3 shows a hierarchical grouping analysis dendrogram (K-means) that allowed verifying the evident dissimilarity of results obtained from the swab (with and without laser and dermis (with laser)), when compared to the other experimental data.

Complementarily to cluster analysis, data was treated by Principal Component Analyses (PCA) method application, permitting the gathering of similar behavior data groups (Figure 4). It basically consists of the diagonalization of a symmetric data matrix, resulting in a new group of variables (principal components), which are linear combinations of the original variables and non-correlated. In this way, a new space is generated in which the variables can be projected and classified into categories or groups. The application of this method allowed the clear differentiation (grouping) between the variables to be verified, highlighting the swab and the dermis (Figure 4A), confirming that the laser treatment promotes results on dermis that show singular behavior when compared





**FIGURE 3** - Cluster Analysis about differentiation of dermis with laser and Swab with and without laser when compared to the other experimental data. Notes: SCL = Swab with laser; SSL = Swab without laser; E1CL = tape strip 1 to 5 with laser; E1SL = tape strip 1 to 5 without laser; E2CL = tape strip 6 to 10 with laser; E2SL = tape strip 6 to 10 without laser; E3CL = tape strip 11 to 15 with laser; E3SL = tape strip 11 to 15 without laser; E4CL = tape strip 16 to 20 with laser; E4SL = tape strip 16 to 20 without laser; EPCL = epidermis with laser; EPSL = epidermis without laser; DCL = Dermis with laser; DSL = Dermis without laser; L10CL = receptor liquid 10 min with laser; L10SL = receptor liquid 10 min without laser, L20CL = receptor liquid 20 min with laser; L20SL = receptor liquid 20 min without laser.

to the other result groups. Figure 4B highlights the differentiation of dermis with laser (DCL) and Swab with and without laser (SCL and SSL), compared to the results set considering all tested concentrations.

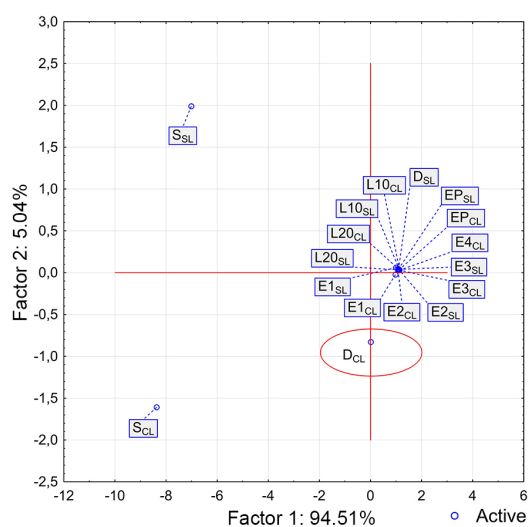
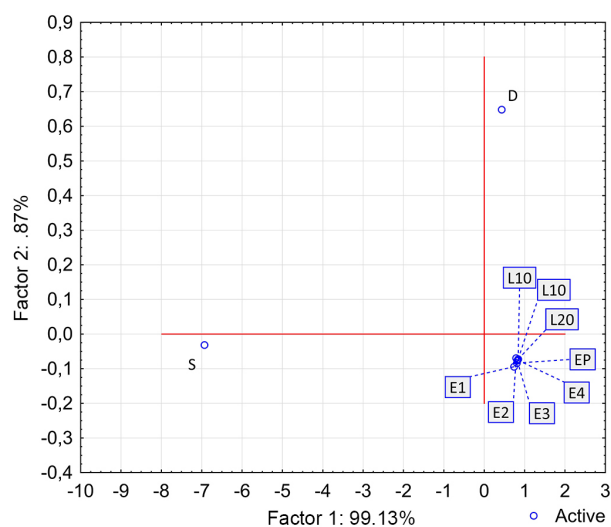
According Yilmaz and Ciltas (2015), diverse methodologies are described in the literature to diclofenac qualitative and quantitative analysis, using many analytical techniques. However, most of them use high performance liquid chromatography with ultraviolet detection (HPLC-UV) (Arcelloni *et al.*, 2001; Bhattacharya *et al.*, 2013). Therefore, this work methodology was developed based on conditions of analysis described on USP 35 (2013) monograph and on the methodology described by Klimes *et al.* (2001).

The method presented suitable specificity as it considered the excipients used in the gel vehicle. Representative chromatograms from samples with or without diclofenac sodium are shown on Figure 5.

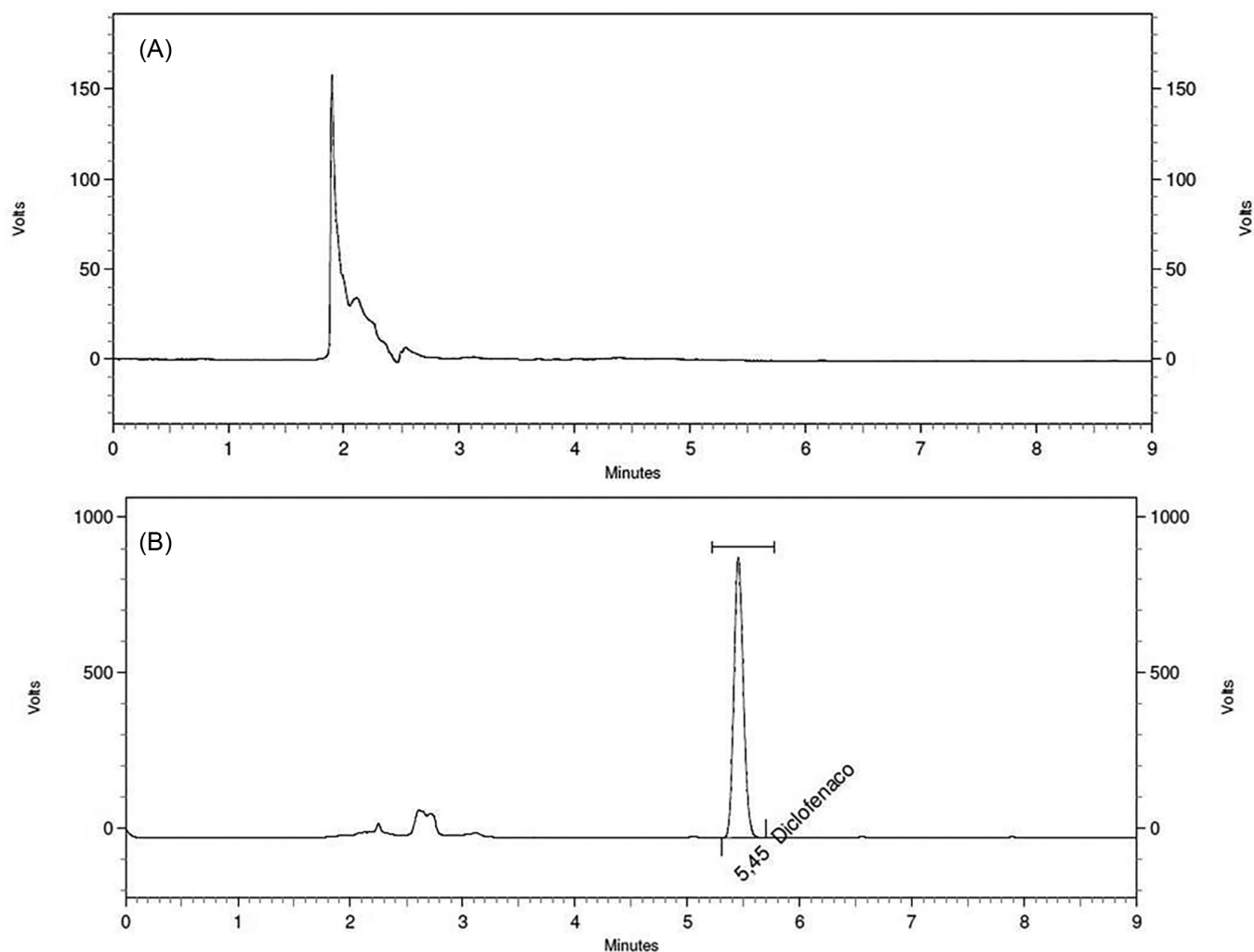
The analytical curve, based on the expected active concentrations on the different skin layers, presented results and Coefficient of Variation (CV) suitable with the aim of the analysis. These analyses were performed in triplicate and their results are shown in Table II.

The obtained coefficient of determination was 0.9966, which shows good explaining ability and linearity coefficient of variation of 4.7% from Detection Limit (DL), determined in  $3.3 \mu\text{g}\cdot\text{mL}^{-1}$  until maximum concentration established in calibration ( $50 \mu\text{g}\cdot\text{mL}^{-1}$ ).

The chromatographic system evaluation parameter values to analyze the standards were: retention factor = 4.2, asymmetry (10%) = 1.16, number of theoretical plates = 15582, indicating chromatographic system adequacy



**FIGURE 4** - Principal Component Analysis method application, allowing the gathering of similar behavior data groups. (A) Differentiation of variables swab and dermis when submitted to laser treatment, (B) differentiation of dermis with laser (DCL) and swab with and without laser (SCL and SSL) compared to the results set considering all tested concentrations.



**FIGURE 5** - Chromatogram analysis obtained from samples without diclofenac sodium addition (A) and samples with diclofenac sodium (B). Chromatographic conditions: chromatographic column ACE® C18 (25 cm x 4.6 mm, 5 µm particle size), mobile phase containing 30% phosphate buffer (pH 2,5) and 70% acetonitrile, 1.0 mL.min<sup>-1</sup> flow, 254 nm detection, 25 µL injected volume and analysis time 9 min.

**TABLE II** - Results obtained from diclofenac sodium solution analysis to build an analytical curve

Concentration (mg.mL <sup>-1</sup> )	Area 1	Area 2	Area 3	Mean ± SD	CV (%)
0.0025	564670	564970	558828	562823 ± 3463	0.6
0.005	734929	742080	737941	738317 ± 2831	0.4
0.0125	2042415	2043344	2053681	2046480 ± 5106	0.25
0.025	3781948	3794774	3786593	3787772 ± 5302	0.14
0.05	7237005	7245341	7855082	7445809 ± 289419	0.4

**Notes:** CV = Coefficient of Variation. SD = Standard Deviations

and compatibility with the USP 35 (2013) recommended parameters. The values of all evaluation parameters to the standards are on Table III.

These results of performance parameters, including specificity, range, linearity, precision (CV), LOD (limit of

detection) and LOQ (limit of quantification), presented by the HPLC method used for the determination of diclofenac sodium in the samples obtained from the permeation tests, assure the sensibility and confidence necessary for the assessment of the data connected with the potential of the

**TABLE III** - Evaluation parameters values to all standard solution analysis

Concentration ( $\mu\text{g/mL}$ )	Retention Factor	Assymetry (10%)	Number of Theoretical Plates
2.5	4.23	1.15	15842
	4.23	1.17	16097
	4.23	1.16	16192
5.0	4.22	1.17	16000
	4.22	1.18	15713
	4.21	1.16	15961
12.5	4.22	1.15	15945
	4.21	1.15	16022
	4.22	1.15	15980
25	4.21	1.16	15742
	4.21	1.15	15712
	4.22	1.16	15745
50	4.22	1.16	15658
	4.22	1.15	15685
	4.37	1.16	15054

CLP to increase the cutaneous permeation of diclofenac sodium.

The performed analysis, in all three investigated concentrations (1.0%, 1.5%, 2.0%) presented the same behavior, as shown on Figure 2. All showed a higher increase of the substance in the dermis with the laser use, suggesting that laser employment in these conditions increases diclofenac sodium penetration and its retention into deeper layers. In all samples (with or without laser application), it is observed that skin surface (swab) showed, as expected, a much higher diclofenac sodium quantity (out of method work range) and that there is no active passage to the receptor liquid, suggesting that diclofenac sodium is not absorbed.

Using an intermediate concentration as a numeric example, it is possible to verify that without laser employment, the analysis representing the first 5 layers from stratum corneum ( $0.049 \text{ mg.mL}^{-1}$ ), layers 6 to 10 ( $0.014 \text{ mg.mL}^{-1}$ ), layers 11 to 15 ( $0.008 \text{ mg.mL}^{-1}$ ) and layers 16 to 20 ( $0.004 \text{ mg.mL}^{-1}$ ) show that the found diclofenac sodium quantity decreases according to the analyzed stratum corneum depth, remaining low in dermis ( $0.011 \text{ mg.mL}^{-1}$ ). As in the samples that underwent laser treatment, the samples that represent the first 5 stratum corneum layers ( $0.024 \text{ mg.mL}^{-1}$ ), layers 6 to 10 ( $0.011 \text{ mg.mL}^{-1}$ ), layers 11 to 15 ( $0.006 \text{ mg.mL}^{-1}$ ) and layers 16 to 20 ( $0.004 \text{ mg.mL}^{-1}$ ) also presented as a result

a decrease in concentrations according to the analyzed stratum corneum depth and a significant increase in the dermis ( $0.117 \text{ mg.mL}^{-1}$ ).

New studies must be conducted with distinct physicochemical properties molecules, aiming to measure the permeation enhancer capacity on different situations. Finally it must be highlighted that, because of operational limitations, this experiment was adapted to evaluate only the effects of laser application on a frozen active solution in a hydrophilic gel, when applied over the skin. According to Bonizzoni (2007), after applying the gel with the laser, skin surface should be exposed to a light beam again by a scanning device, which could have contributed to the permeation process if it had been used in this experiment.

## CONCLUSION

The results indicate that the Cryo Laser Phoresis technique, when used under the conditions described in this study, is able to enhance skin permeation of diclofenac sodium and potentially of other molecules with similar physical-chemical proprieties, thus constituting an interesting alternative to drug administration, especially in situations in which penetration in deeper skin layer is necessary and where the systemic use may be unfeasible or may be capable to promote unpleasant reactions.

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