

Thermodynamics of Molecular Recognitions between Antineoplastic Drug Taxol and Phosphatidylcholine

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ABSTRACT

The aim of this study was to study the basic features of Taxol recognition with phospholipids by applying the thermodynamic and spectroscopic measurements. The obtained information could be used further for deductions on its precise cellular and pharmacological mechanisms of action, on improvements of its solubility properties by phospholipids, as well as for designing the novel lipidic carriers for drug delivery.

Key words: Antineoplastic agents, chemotherapy, Taxol, phosphatidylcholine, Taxol-membrane interactions, membrane fluidity

INTRODUCTION

Over the past two decades, among the several new chemotherapeutic agents, the taxanes have played a significant role in the treatment of various malignancies (Singla et al. 2002; Stohs, 2005; Hennenfent and Govindan, 2006; Safavy, 2008). These are a group of hydrophobic antineoplastic drugs, approved by Food and Drug Administration (FDA) to cure breast, ovarian, non-small-cell lung and prostate cancers (Stohs, 2005). As a member of this group, Taxol was discovered in 1960s within the frame of a National Cancer Institute study for screening the natural compounds with anticancer properties (Wall and Wani, 1995a; 1995b). It was identified as the crude extract from the bark of the North American pacific yew tree *Taxus brevifolia*, subsequently found to be effective against various tumors (Stohs, 2005). Unfortunately, its clinical testing was unsatisfactorily delayed due to limited sources of the pacific yew tree bark and its poor solubility

(Harlan, Jr., 2001; Wall and Wani, 1995a,b; Stohs, 2005). Therefore, the tedious procedure of the total synthesis of Taxol has always been a challenging target of a number of research groups as an improved source of this promising anticancer drug (Zefirova et al. 2005).

Taxol (Paclitaxel) is a complex natural alkaloid diterpene compound with a molecular weight of 853 (amu) and is comprised of tetracyclic core (baccatin III) and ester-linked side chain attached to the 13th carbon of the latter. Pharmacological targets of the drug are cellular microtubules with binding sites engaged, which biological functions are not yet clarified. Application of Taxol in cancer chemotherapy has been limited by its low aqueous solubility. Since this is regarded as an important issue for drug formulation, various solubilizing systems have been explored to improve its poor solubility. Among these, several approaches such as using co-solvents or emulsions, designing its new prodrug or analog forms as well as developing liposomal and

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micellar preparations of Taxol have been extensively tried (Nuijen et al. 2001; Singla et al. 2002; Safavy, 2008). However, none of these approaches has been satisfactory enough to be introduced to the clinical practice, mostly because of the lack of biocompatibility to meet the requirements of intravenous preparations. Of these, the use of lipidic carriers in the form of emulsions (Nornoo, 2008) nanoscale lipocores and liposomes (Terwogt, et al., 1997; Nuijen, et al. 2001; Singla et al. 2002; Castor, 2005; Safavy, 2008) for increasing the drug solubility are one of the most promising, but still awaiting further characterization.

In this respect, the objective of this study was to follow further the molecular recognitions between Taxol and phosphatidylcholine-one of the major components of eukaryotic cell membrane phospholipids. The goal to be achieved is two-fold-both cell biological and biotechnological aspects are aimed. By further clarifying the precise mechanisms of Taxol-lipid interactions, better understanding of its pharmacological activities can be obtained, as well as designing the novel lipid based drug formulations with improved bioavailability properties would be possible. Since most of the commercial preparations of Taxol for intravenous infusion contain ethoxylated castor oil (Cremophor EL), it is interesting to study the pharmaceutical and physicochemical behaviour of the drug in similar solubilizing environments. Thus, well tolerated lecithin was chosen as a model emulsifying agent to simulate the parenteral formulation. The employed egg lecithin could be a good approach to currently used micellar solutions of egg lecithin and cholic acids as carriers for fat-soluble vitamin E (Cernevit) and vitamin K (Konakion MM) (Sznitowska et al. 2008). Having appreciated the importance of various physical forms of Taxol, possessing different therapeutic potentials, thermal analysis best fits for studying its solid states. More specifically, information on the physical states of drugs inside micelles or liposomes is useful in predicting formulation properties such as drug-release biodynamics and kinetics. Such loading into micelles or liposomal entrapment often leads to drug crystallization, whereas the drug molecules exist in molecularly dispersed state at low loading. To better understand these phase transitions, a thermodynamic approach to follow Taxol-lipid recognitions is presented herein.

MATERIALS AND METHODS

Materials

Egg phosphatidylcholine was purchased from Avanti Polar Lipids (Alabaster, AL, USA). FTIR-grade KBr (22.186) and Paclitaxel were a product of Sigma Chem. Co., MI (USA). All the chemicals used were from the highest analytical grade.

Methods

Differential Scanning Calorimetry

Thermal analyses were carried out using Perkin-Elmer Pyris differential scanning calorimetry (DSC) instrument. Previously weighed and dried Taxol-lipid mixtures in desired ratios were placed in a hermetically sealed aluminium pans. Both the lipid and paclitaxel were dissolved in chloroform forming the final ratios and placed in aluminium pans prior to the measurements. The lipid concentration used throughout the measurements was 20 mg/ml. As a control, a pan containing the dried paclitaxel of the same amount was prepared. Paclitaxel was dissolved also in chloroform for comparative purposes. The cell was purged with Argone and all the measurements were made with a scan rate of 10°C/min.

FTIR Spectroscopy

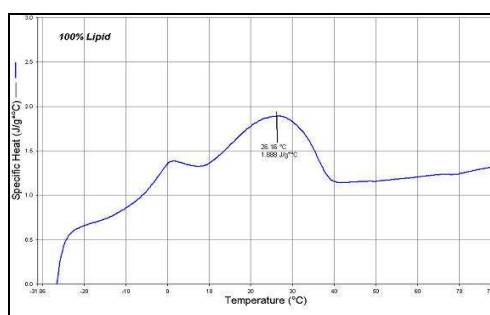
Infrared spectra were recorded on IFS 66/S FTIR spectrometer (Bruker Analytische Messtechnik GmbH, Karlsruhe, Germany), equipped with He-Ne laser detector and KBr beam splitter. KBr pellet method was employed as FTIR sampling technique. The samples were prepared by mixing the lipid and drug in the desired ratios and pressing the mixtures with a die press. Spectra were collected after short incubation of lipid with Taxol. Interferograms were accumulated over the spectral range 4000 cm^{-1} to 400 cm^{-1} , with a nominal resolution of 2 cm^{-1} and a minimum of 320 scans. The criterion for the elimination of water effect from the spectra was based on the straight baseline between 1750 cm^{-1} and 2200 cm^{-1} , where the water combination mode was located. As a control, the spectra of unbound Taxol was taken and compared with those reported in the literature previously. Afterwards, the spectra of egg phosphatidylcholine was recorded as the following. After the normalization of absorbance and baseline correction, the peak frequencies of the symmetric CH_2 stretching, the asymmetric $\text{P}=\text{O}$ stretching and the asymmetric $\text{N}-(\text{CH}_3)_3$ stretching peaks

were determined by using the original software provided by the manufacturer. FTIR spectra were taken for each single component engaged in DNA-lipid complex formation for all the combinations of binary mixtures Taxol-phosphatidylcholine in various ratios for comparison.

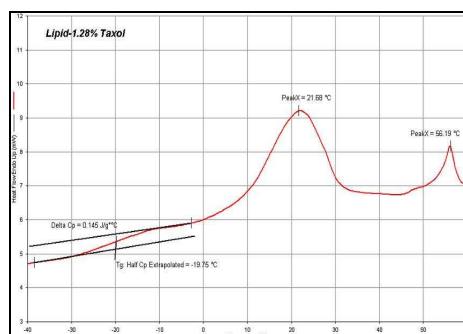
RESULTS AND DISCUSSION

The aim of this study was to investigate how Taxol recognized and bound to phospholipids and how it affected the packing and fluidity of membranes. The thermograms of DSC measurements could

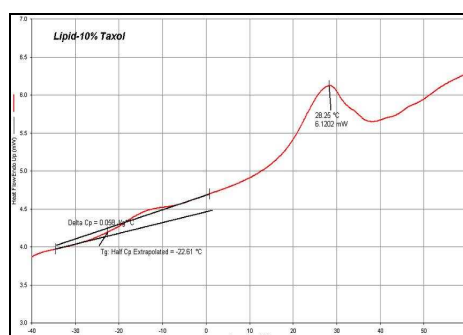
distinguish between the phospholipid gel and liquid crystalline phases. As the calorimetric data from the heating curves reflected essentially the same changes as those from the cooling curves, only endothermic curves were used to characterize the thermotropic phase transitions of the binary drug-lipid mixtures. It was very interesting to study the excess drug effects by varying the drug concentration and keeping the lipid concentration fixed. This would give further insights into the concentration dependent Taxol effects, as well as into possible mechanisms of membrane deformation.



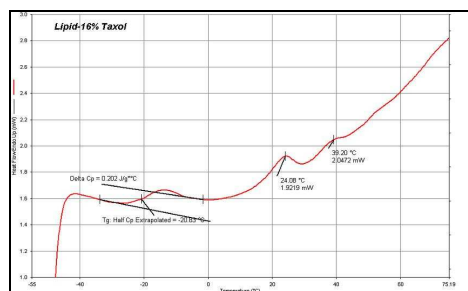
(a) A melting curve of a pure unbound phosphatidylcholine.



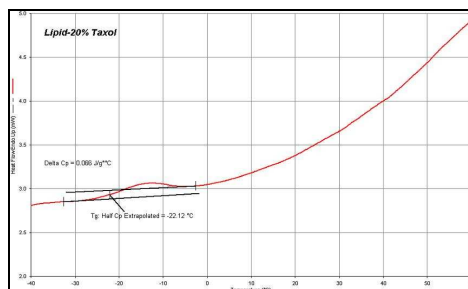
(b) A DSC thermogram depicting the melting profile of 1,28% drug/lipid mixture.



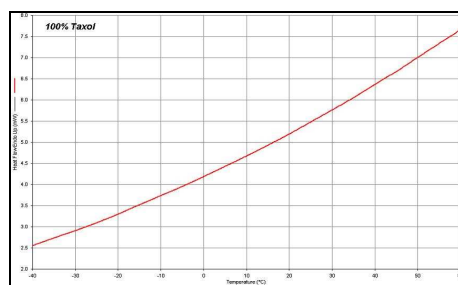
(c) A thermal melting profile of 10% drug/lipid mixture.



(d) A DSC thermogram showing the phase behaviour of 16% drug/lipid mixture.



(e) A phase behaviour of 20% drug/lipid mixture.



(f) A DSC scan of a pure unbound Taxol.

Figure 1 - DSC thermograms of unbound Taxol and its various mixtures with egg phosphatidylcholine in the desired ratios, as depicted. The thermodynamic parameters are assigned automatically by the Pyris software of the DSC instrument. The samples were prepared as mentioned in the Materials and Methods.

Fig. 1 shows the endothermic phase transitions for binary mixtures of egg phosphatidylcholine and Taxol. Information on the physical state of drugs entrapped in micelles or in liposomes is very useful in predicting and designing improved formulation properties such as drug release kinetics from vesicles. The high loading of a drug with poor aqueous solubility, such as Taxol into vesicles usually leads to its crystallization, whereas the drug molecules exist in molecularly dispersed form at low loading profiles. Thermal analysis best fits for examining the crystallization features in simulated lipid environments. The first thermogram in Fig. 1 shows the heating behaviour of phosphatidylcholine alone, followed by several

DSC scans of Taxol-lipid complexes in various ratios in the solid state. All the thermograms differed from the heating characteristics of Taxol alone in the last thermogram, which showed no transitions at all, since it melted at much higher degrees at 216°C. This suggested that the drug was homogeneously and molecularly dispersed within the surrounding lipid. Obviously, this recognition with lipid molecules affected the crystalline structure of Taxol in a hermetically sealed aluminium pans.

In general, the addition of the drug induces certain perturbations or more specifically leads to microdomain formation of phospholipid molecules. When added even at low concentration

to phosphatidylcholine, it gives rise to shift of the glass transition temperature (T_g). The appearance of a second peak at 56.19°C indicated the formation of another phase. Obviously, drug-induced microdomain formation occurred. Since such a phase transition was highly sensitive to existence of foreign molecule bound to polar parts of phospholipids, the changes in T_g could not be explained only by specific molecular transitions. In 10% concentration, Taxol shifted the main phase transition temperature (T_m) from 26.16 to 28.25°C (Fig. 1). However, the surrounding thermogram remained symmetric. On the other hand, the T_m peak narrowed and its height diminished. When used at its lowest concentration, the drug shifted T_m to lower degrees from 26.16 to 21.68°C . However, the surrounding thermogram peak remained symmetric, while its width was narrowing. This effect increased the T_m cooperativity of the phase transition and restricted the flexibility of phospholipids. In such a case, the highly ordered all-*trans* hydrocarbon phospholipid chain conformation existed. *Gauche*-(kinked) conformation, which leads to higher rotational freedom did not exist. The addition of 10% Taxol shifted the main phase transition temperature, giving rise also to appearance of a smaller second peak. This indicated that in higher amounts, the drug increased its affinity of binding to the phospholipids. In comparison with T_m , sharper changes were seen in glass transition temperature

(T_g). Thus, in the presence of lower amounts of Taxol, the latter shifted from -19.75 to -22.61°C , while extending the peak width. It was interesting to note, that the same effect was observed when 10, 16 and 20% concentrations of the drug were used (Fig. 1). These effects showed that when used in 1-10% concentrations, the drug increased the phospholipid fluidity by lowering T_m and increased its cooperativity by narrowing the phase transition peak. The most profound effects were seen in the presence of 10% Taxol, where T_m increased and a second peak disappeared. On the other hand, the presence of 16% Taxol again lowered T_m , thus leading to re-appearance of the fluid phase. When added at 20%, the drug affected only the glass transition temperature. Thus, in higher amounts, Taxol fluidized the phospholipid dispersion. In these circumstances, the glass transition temperature was more informative than the main phase transition temperature. These results were due to the chemical nature of the employed egg phosphatidylcholine and from the spatial properties of Taxol. Being a bulky molecule, the drug could not reach the inner parts of phospholipid hydrocarbon chains. It had only a limited access to hydrophobic parts and apparently bound to their surface acyl chains. The validity of this deduction remains to be tested further by employing for instance Electron Spin Resonance spectroscopy.

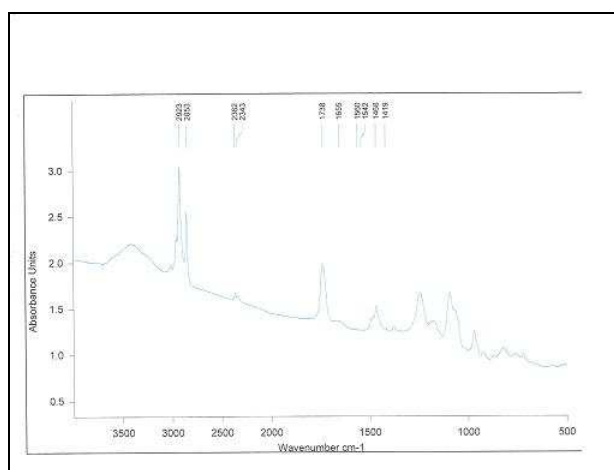


Figure 2 - Overall infrared spectrum of egg phosphatidylcholine.

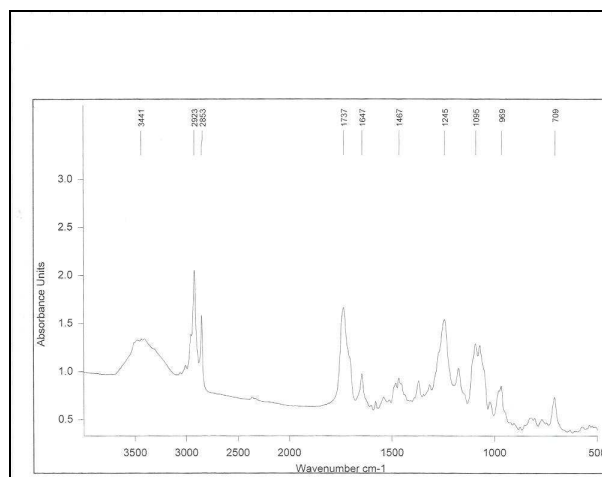


Figure 3 - The infrared spectrum of equimolar mixture of Taxol with egg phosphatidylcholine.

Having considered the advantages of vibrational spectroscopy over the other analytical methods for the analysis of drug-membrane phospholipid interactions (Günzler and Gremlich, 2002), the Fourier Transform Infrared Spectroscopy (FTIR) was applied for further characterization of molecular recognitions between Taxol and phosphatidylcholine. The most common method of sample preparation for Fourier Transform Infrared Spectroscopy is solid state analysis of molecules under study after their compression and mixing with KBr. In their study, Meyer et al. (2004) showed that the compaction of the KBr/sample mixtures did not foster the aggregation and remained conformationally unaltered by this process. The method is invaluable in determining the role of different functional groups engaged in such complexations (Seydel and Wiese, 2002). Fig. 2 and Fig. 3. show the overall infrared (IR) spectra of unbound drug and its equimolar mixture with the phospholipid, respectively. Since, using the excess quantities of Taxol created a drug dominated IR spectra of the binary mixtures (data not shown for brevity), only 1:1 mixture has been presented here, because it gave better impression of the recognition effects.

Under these conditions, the amorphous Taxol was converted to anhydrous state, suggesting that several solid-state structures of the drug coexisted. Major lipid specific band frequencies were seen when equimolar ratios of drug-lipid complexes were used. The most important of these were those belonging to CH vibrations ($2750\text{--}3100\text{ cm}^{-1}$) and CH_2 wagging progression and the CH_2 scissoring vibrations ($1150\text{--}1400\text{ cm}^{-1}$ and $1465\text{--}1475\text{ cm}^{-1}$).

These depicted the conformational order and provided information on packing effects of the acyl chains, respectively. PO_2^- vibrations were located at 1242 cm^{-1} . On the other hand, Taxol possessed substantial bands at $1600\text{--}1750$, $1180\text{--}1300$ and $630\text{--}770\text{ cm}^{-1}$. These were seen in the spectra of various drug-lipid mixtures, suggesting a drug dominated spectrum, indicating their recognition and binding. In comparison with the spectra of the unbound drug the lipid-bound spectral shifts of Taxol's carbonyls from 1736 cm^{-1} to 1732 cm^{-1} and from 1736 cm^{-1} to 1707 cm^{-1} were seen (Fig. 3 and Table-1). These were retained also in higher drug ratios. The strong bands at $3300\text{--}3500\text{ cm}^{-1}$ were due to OH-groups linked to the H-bonds. Following the drug-lipid recognition, the intensities were decreased and additional band shifts took place. This indicated a conformational restriction of lipid moiety due to bond formation with the drug, depicting the decrease in the drug flexibility. In conclusion, FTIR spectroscopy clearly showed that Taxol-lipid recognition and binding was governed by CH and CH_2 groups, as well as H-bonded surface OH-groups. In addition, PO_2^- , C=O, C=C and CH_2 groups of the drug were also engaged. Data showed that Taxol fluidized the upper region of the acyl chains, whereas the hydrophobic core was rigidized. The increase in the asymmetric and symmetric methylene stretching frequencies, the splitting of methylene scissoring band and broadening of carbonyl stretching mode depicted that the drug mostly recognized the cooperativity region, bound to the surface phospholipid acyl chains and induced fluidity in their headgroup

region. At higher amounts ($\geq 10\%$) it located at the interface and eventually formed a phase separation, resulting in crystallization, as deduced also from DSC measurements (Fig. 1).

Thus, by employing such a calorimetric and spectroscopic approaches, further details of Taxol-membrane phospholipid interactions could be obtained and exploited for elucidating its chemotherapeutic effects. Therefore, studying its recognition events with cellular phospholipids becomes crucial. Such biophysical and structural studies of Taxol-lipid arrangements can give valuable information about the organization of the

drug in the membranes of both normal and malignant cells and can help to optimize the lipid matrix concerning its solubility potential. Moreover, the question of how higher amounts of the drug give rise to membrane deformation could be clarified in more detail. In this respect, a novel hypothesis can be generated regarding the fact that concentration dependent Taxol-induced membrane deformation may require physical perturbation of the lipid bilayer, a process in which the role of lipophilic drugs that partially penetrate the lipid bilayer is to be emphasized.

Table 1 - Principal infrared absorption bands, relative intensities and frequency assignments (cm^{-1}) for free lipid and its binary complex with Taxol.

| Phosphatidylcholine | Vibrational frequencies | Corresponding moieties |
|------------------------------------|-------------------------|--|
| | 3420 | water band |
| | 2923 | CH stretching |
| | 2853 | CH stretching |
| | 2382 | $\nu_s[(\text{CH}_3)_4]$ |
| | 2342 | $\nu_s[(\text{CH}_3)_4]$ |
| | 1738 | $\nu_s[\text{C}=\text{O}]$ |
| | 1556 | $\delta[\text{C}-\text{H}]$ |
| | 1550 | $\nu_{as}[\text{PO}_2^-]$ |
| | 1419 | scissoring $\delta[(\text{CH}_2)_n]$ |
| Phosphatidylcholine- Taxol complex | | |
| | 709 | Finger print |
| | 969 | Assymmetric $[\text{N}^+(\text{CH}_3)_3]$ stretching |
| | 1095 | Symmetric $\nu_s[\text{PO}_2^-]$ |
| | 1245 | Antisymmetric $\nu_{as}[\text{PO}_2^-]$ |
| | 1467 | Scissoring $\text{CH}_2\delta$ (hexagonal) |
| | 1647 | $\text{C}=\text{O}$; symmetric alyl $\text{C}=\text{C}$ |
| | 1737 | $\text{C}=\text{O}$ stretching |
| | 2853 | Symmetric $\nu_s[(\text{CH}_3)_4]$ |
| | 2923 | Symmetric $\nu_s[(\text{CH}_3)_4]$ |
| | 3441 | H-bound OH groups |

ACKNOWLEDGEMENTS

This work was supported by Gazi University Research Foundation (Project No: 02-2005/15). The author greatly acknowledges the facilities and personnel of The Central Laboratory of Middle East Technical University (Ankara-Turkey) for access to instruments.

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Received: February 06, 2009;

Revised: October 19, 2009;

Accepted: June 27, 2010.