








Use of scanning electron microscope to evaluate the marginal fit of protocol bars obtained through benchtop or intraoral digital scanners

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Aim: To evaluate the marginal fit of protocol bars milled from digital models obtained by conventional molding followed by bench scanning or digital molding with an intraoral scanner.

Methods: Four morse-cone implants and the mini-pillars were installed in a 3D printed mandible model (master model). Digital models of the master model were obtained by (n=10): (Group A - Conventional) conventional (analog) molding of the master model followed by bench scanning or (Group B - Digital) molding of the master model with an intraoral scanner. All-on-four protocol bars were designed and milled from the digital models for both groups and screwed into the master model. Scanning electron microscopy (SEM) images from the distal, central, and mesial regions of each implant were obtained and the implant-protocol bar marginal fit was measured in an image software (Image J). The mean misfit of each region was analyzed by two-factor ANOVA, Tukey test, and Student's t-test (0,05 = 0.05). **Results:** The digital approach (B) showed higher misadaptation than the conventional approach (A, $p < 0.05$), regardless of the region evaluated. In group A, the central region showed higher maladjustment than the mesial region ($p < 0.05$), however, there were no differences among regions of group B ($p > 0.05$).

Conclusion: The conventional method of acquiring digital models using the bench scanner produced bars for the All-On-Four protocol with better marginal fit than the digital models obtained with an intraoral scanner.

Keywords: Dental implants. Computer-aided design.

Introduction

Studies show that patients undergoing partial or total rehabilitation with dental implants have a predictable and favorable success rate¹⁻³. Nevertheless, after completion of the surgical procedure, the success of the treatment occurs only with the proper installation of the definitive prosthesis. However, the prostheses need to be made using a correct sequence and high-quality standard so that a passive and precise adjustment of the connection with the implant occurs³, as the lack of adaptation of the prosthesis on the implant can generate minor consequences such as distortion and loosening of the fixation screw, to serious problems, as crown fractures or implant failure⁴.

Passive fit is achieved by simultaneous contact between the structure and the implant or abutment surface. Therefore, this adaptation is essential to avoid stress accumulation at the bone/implant interface, preserving osseointegration and ensuring the longevity of the treatment⁴. In the search for the perfect fit, producing dental molds and/or implants with excellent precision became necessary. Therefore, high-quality molding became critical to the treatment sequence and, consequently, to achieving success⁵.

In protocol-type prostheses, commonly used in full-arch rehabilitation, the position and angulation of the implants have meaningful influence and importance at the time of molding⁶. These variables influence the decision for the material type and the geometric shape of the bars, and the use of a material capable of absorbing and dissipating the stresses applied to the implants during function⁷. In this sense, the evolution of materials and molding techniques along with the evolution of intraoral scanners has raised concerns about which technique would be the best for acquiring the final model. For some reasons, such as financial, the first option for clinicians is still the conventional method (molding). But the decision depends on several factors since it requires a significant number of materials and techniques, generating a grander number of steps, increasing the demand for digital systems⁸.

To determine whether the seating of the protocol-type bar occurs passively and without misfits, accurate tests must be performed to measure the presence of gaps in different regions of the prosthesis-implant connection. In this sense, the scanning electron microscope (SEM) is the tool commonly used to measure the accuracy of the gap generated between the connection of the prosthetic element with the surface of the abutment or dental implant, due to the precision of the analysis generated by the magnification of the image obtained⁹.

In the face of the existing doubts and lack of consensus in the literature regarding the effectiveness of the benchtop scanner or intraoral scanner to determine the seating accuracy and adaptation of all-on-four protocol-type bars milled from virtual models, studies that evaluate the marginal fit of bars milled by both methods are required. Thus, the aim of this study was to evaluate, by means of scanning electron microscopy, the adaptation of milled protocol-type bars obtained after scanning with a benchtop scanner or intraoral scanner. The null hypothe-

sis was that there would be no significant difference between the adaptation of milled protocol-type bars obtained after scanning with a benchtop scanner or intraoral scanner.

Materials and Methods

The study was submitted to the Research Ethics Committee (CEP PROTOCOL 2018/0968) of the Faculty and Research Institute of São Leopoldo Mandic and was dismissed for not involving humans or animals.

Master Model Fabrication

One (01) jaw mannequin (master model) was made using software (Exocad 2.2) and a 3D printer (Miicraft 125 Ultra - Smartdent)^{6,10}. Four morse taper implants (3.5 diameter and 13 mm length, Unitite, SIN Implants System) were installed on the mannequin, by only one experienced operator¹. A mini-abutment compatible with the morse taper system (SIN Implants system), with a standardized height of three millimeters, was installed on each implant.

Preparation of the specimens

For the preparation of the specimens, protocol bars on the implants, digital models of the implants positioned in the master model were obtained by conventional molding (analog) followed by scanning with a benchtop scanner (Group A), and another digital molding was obtained by the intraoral scanner directly in the master model (Group B)⁸ (n=10):

Group A: Conventional. Starting from the point after installation of the mini-abutments on the implants, the molding transfers (SIN Implants System) were installed and splinted with metal rods associated with self-curing acrylic resin (Pattern - GC)^{6,3,11}. The open tray molding technique was used associated with polyvinyl siloxane impression material (Express XT - 3M Oral Care)^{10,12,13} (Figure 1A and B). The impression material was handled according to the manufacturer's instructions and inserted into the open tray. After polymerization of the material, the set was removed from the mannequin and the analogs were installed by the same operator who installed the implants. The special plaster (FujiRock - GC) was poured and the time required for the plaster to crystallize, generating the working model, was allowed. This model was inserted into the benchtop scanner (Bioscan - Bioart) creating a digital STL file for drawing the protocol bar and milling (DM5 - Tecnodrill)¹¹.

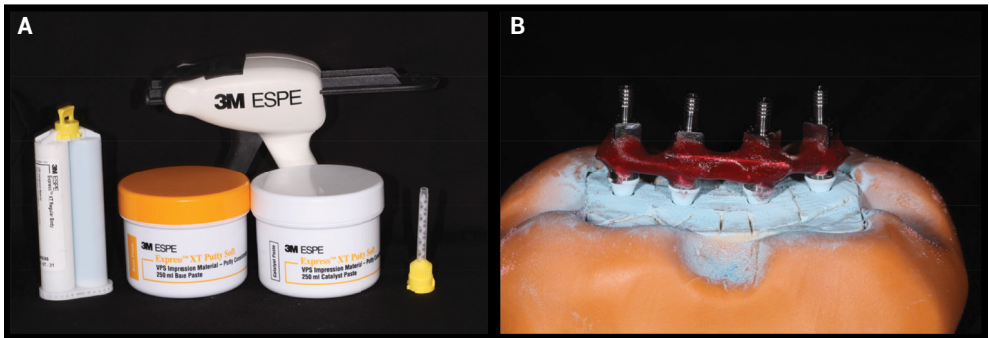


Figure 1. Impression material (A) used in the transfer molding of group A and transfers splinted on the working model (B).

Group B: Digital. The digital model was acquired after installing four standard scanning bodies (Scanning JIG JBMMA - SIN Implants System) for each mini-abutment and performing the scanning process with an intraoral scanner (Omnicam - Dentsply Sirona). The STL file went to the same responsible technician who designed the protocol bar and sent it to milling (DM5 - Tecnodrill)¹¹.

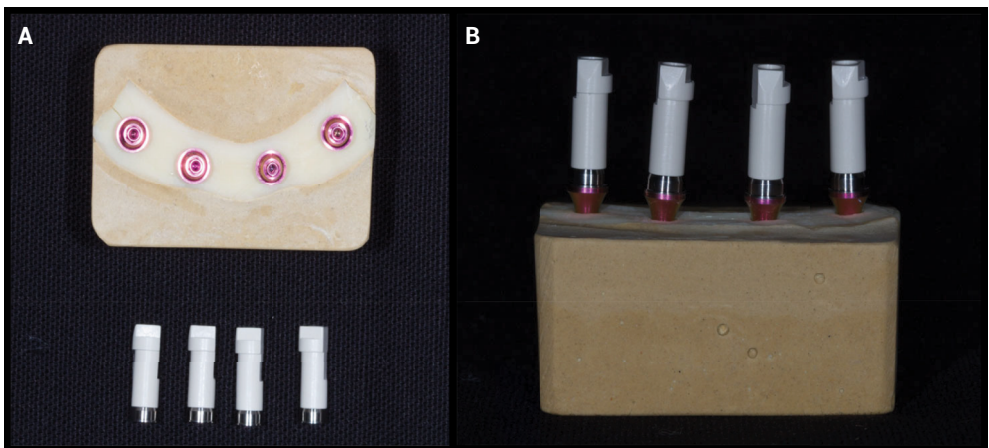


Figure 2. A master model with implants installed and scan bodies (Scan JIG) (A), is used to perform intraoral scanner scanning directly on the master model. A master model with specimens installed for intraoral scanning (B).

The files were sent to the laboratory and an experienced CAD operator designed the twenty bars (Groups A and B) in square format⁷ in CAD software (Exocad 2.2), and the bars were milled in titanium (DM5, Tecnodrill).

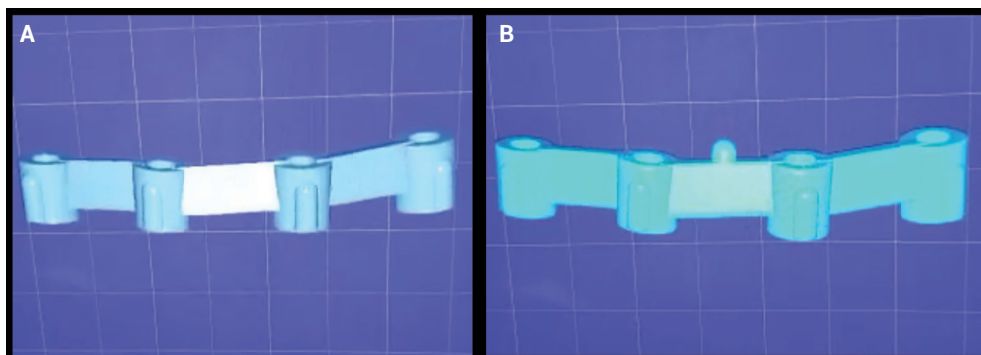


Figure 3. Digital drawing of bars. (A) Drawing of the bar of group A (conventional) and (B) drawing of the protocol bar of group B (digital).

An experienced operator inserted each bar into the original master model, screwing each connection with a torque of 15N, measured with a calibrated torquemeter.

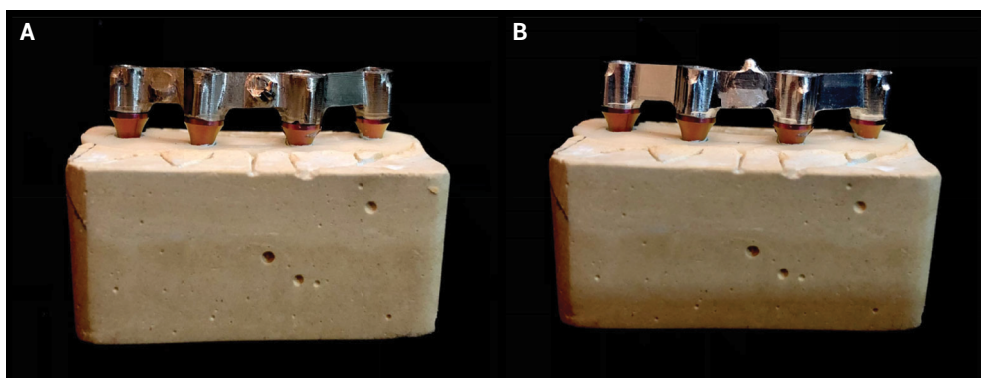


Figure 4. Milled bars on the master model. (A) Milled bars of group A (conventional) and (B) Milled bars of group B (digital) adapted in the master model.

Scanning Electron Microscopy (SEM) and Marginal Fit Analysis

The SEM analysis (JEOL-JSM, 6460LV, Tokyo, Japan) was performed on each of the protocol-type bars⁴, in the distal, central, and mesial regions, generating twelve images of each protocol-type bar specimen. The SEM operated at 15kV in high vacuum mode and 45 Pa. This method was selected because it allows measuring the adaptation of the milled bar/mini-pillar interface using electrons that create images with a high degree of magnification and resolution¹⁴.

The images obtained were transferred to the imaging software (ImageJ software, US National Institutes of Health, Bethesda, Maryland, USA) to determine the length of each gap segment. The SEM image scale bar, at $\times 500$ magnification, was used for distance calibration. The width of the gap was defined as the straight-line distance between the milled bars and the implants¹⁵. In the Image J

software program, a line between two points of known distance (the scale bar of the SEM) was set as the measurement scale (pixel: length relationship known). Three linear measurements were made (in μm) of the vertical gap between the milled bars and the implant in each of the regions evaluated (distal, central, and mesial), and the mean values obtained from these three regions were submitted to statistical analysis.

Statistical Analysis

The normality of the data was confirmed by the Shapiro-Wilk test, and an outlier was removed from Group A, in the mesial region. Data were submitted to two-way Analysis of Variance (ANOVA, factors: *group* and *region*) and Tukey HSD Test. Additionally, Student's t-test was performed for independent samples (comparison among groups). All analyzes were performed using the Statplus software: mac (AnalystSoft, v.6), with a significance level of 5%.

Results

Table 1 describes the mean values (in μm) and standard deviation of the measurements performed on each implant, and on each protocol bar, according to the regions of the protocol bar and implant connection (distal, central, and mesial) and groups (A: conventional and B: digital).

Table 1. Mean (in μm) and standard deviation of the measurements performed on each implant of each protocol bar, in the distal, central and mesial regions, according to the methods for obtaining the metallic structure (Group A: conventional and B: digital).

Regions	Groups	
	Group A Conventional	Group B: Digital
Distal	18.7 (7.6) Bab	40.1 (10.8) Aa
Central	28.8 (10.5) Ba	46.1 (13.1) Aa
Mesial	13.1 (2.9) Bb	38.4 (8.6) Aa

Caption: Means followed by distinct letters are statistically different according to two-way ANOVA and Tukey's HSD test ($p < 0.05$). Capital letters compare groups A and B in each region (rows), and lowercase letters compare regions in each group (columns).

The results indicate that group B showed greater misadaptation than group A ($p < 0.05$), regardless of the region evaluated. In group A, the central region showed greater misadaptation than the mesial region ($p = 0.0116$), but the central and mesial regions did not differ from the distal region ($p > 0.05$). Group B exhibited no differences among the evaluated regions ($p > 0.05$).

Additionally, the overall mean of each group was compared, regardless of the region evaluated. It was observed that treatment B presented greater misadaptation than group A (Table 2).

Table 2. Overall mean (μm) and standard deviation (sd) marginal fit measurement of each implant, regardless of the region evaluated.

Groups	Overall mean (sd)	<i>p</i> value
A (Conventional)	21.6 (7.7) B	0.000474
B (Digital)	39.2 (11.9) A	

Caption: Mean values followed by distinct letters indicate statistically significant differences according to the t test ($p < 0.05$).

The SEM images of the protocol-type bar interface on implants (Fig. 5) obtained using a benchtop scanner (A, B, and C) or intraoral scanner (B, D, E), illustrate the regions evaluated and measured for misfit (distal - A and D; central B and E; mesial C and F). The central region (B and E) indicates the existence of a gap, observed in all specimens for both groups. Image D (Group B) demonstrates, in addition to gap formation, overcontour of the metal bar, while in F (Group B) an undercontour is associated with gap formation. Representative images were obtained at $\times 500$ magnification.

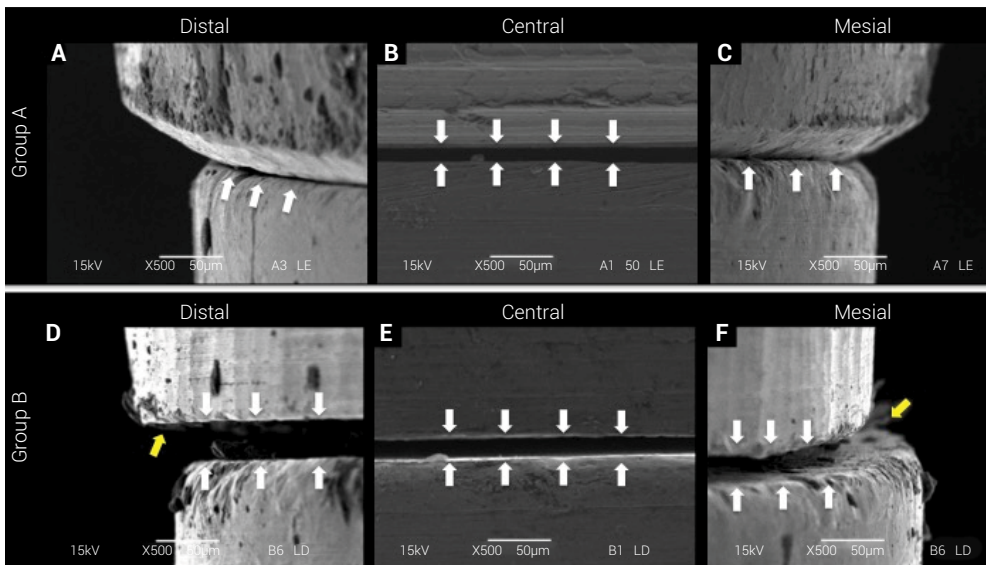


Figure 5. Representative scanning electron microscopy (SEM) images of the all-on-four protocols on implant attachments, produced by a benchtop scanner (A, B, and C) or intraoral scanner (D, E, F), according to the regions evaluated (distal - A and D; central B and E; mesial C and F). White arrows indicate the gap regions measured in the Image J software, and yellow arrows correspond to the over- (D) or under-contour (F) region of the metallic structure. (Magnification: $\times 500$)

Discussion

The objective of this study was to evaluate, by means of scanning electron microscopy, the marginal fit of milled protocol bars after the acquisition of the scan with a benchtop or intraoral scanner in models acquired from conventional moldings. The results indicate that the All-on-Four protocol bars obtained by benchtop scan-

ning showed greater adaptation than those obtained by intraoral scanning. Thus, the null hypothesis that there would be no difference between the groups evaluated was rejected.

In recent years, authors have reported the difficulty in rehabilitating patients with protocol-type prostheses, especially the challenge of obtaining passive seating, since the materials used during the process produce uncontrollable variations that directly reflect the result. Since then, the evolution of techniques involving implant-prosthesis is constant, and technology has a fundamental role in the current form of All-on-Four rehabilitations². In this sense, the main challenges of CAD/CAM systems are to reproduce the quality of products and compete with analog techniques⁶.

It is known that for an All-on-Four rehabilitation to be successful in the long term, one of the fundamental factors is the adaptation of the bar that supports the entire dental structure. Balouch et al.¹⁶ compared the three-dimensional accuracy between moldings with open tray and closed tray and concluded that the closed tray technique exhibited superior performance. Nakhaei et al.¹⁷ compared the three-dimensional accuracy of moldings with open and closed trays. After generating a total of 42 models, the authors observed that the impression technique with an open tray showed greater precision compared to a closed tray, and this information was confirmed in a literature review carried out with more than 417 articles¹². Thus, to select the most accurate impression technique, transfer molding with an open tray was selected for Group A. Although it has been demonstrated that the open-tray molding technique presented greater accuracy¹², the authors indicated that intraoral scanning for 3D model acquisitions was a reality and that its use by clinicians was on the rise. According to these authors, intraoral scanning could promote better results than moldings with closed trays and compatible with results with open trays.

The present study confirms previous observations in which researchers¹⁸ compared intraoral scanning as an alternative technique to conventional molding with an open tray associated with polyvinyl siloxane, an addition-reaction silicone elastomer. According to the results¹⁸, conventional impression promoted better marginal fit than intraoral scanning, confirming that conventional impression is superior to intraoral scanning. These results were corroborated by Alsharbaty et al.¹⁹, in which the authors compared conventional molding with polyvinyl siloxane to intraoral scanning techniques and confirmed that conventional molding promotes more accurate clinical results than intraoral 3D image acquisition.

In another research, Huang et al.²⁰ evaluated the accuracy of intraoral and benchtop scanning methods, similar to the methodology used herein. A mannequin with four implants and four mini abutments installed on the implants was used. After acquiring the master models files through scans with an intraoral scanner or with a benchtop scanner on the models generated through conventional molding with an open tray and polyvinyl siloxane, the researchers showed that conventional moldings with open trays are more accurate than the intraoral scan. Besides, it should be noted that acquisition methods also influence the accuracy of implant-supported All-on-Four rehabilitations. Stimmelmayer et al.¹¹ compared the discrepancy between two different impression techniques of All-on-Four implants and concluded that the splinted pick-up technique should be used for impressions. The authors also stated

that clinicians need to choose a technique that they feel capable, confident in, and safe to perform.

Contrarily to these findings, a previous research⁸ evaluated the performance of conventional moldings and digital acquisitions of implant-supported prostheses in 25 patients treated with the All-on-Four technique associated with immediate loading for one year. The authors concluded that it is possible to manufacture satisfactory accurate prostheses on implants using digital impression techniques⁸.

Pesce et al.²¹ evaluated the gaps of printed protocol bars with the images acquired through an intraoral scanner and concluded that these protocol bars are reliable for a passive adaptation point. However, the authors reported that the experience of the intraoral scanner operator is critical to the clinical outcome²². Therefore, it is important to note that some studies that do not report whether the operator has experience in handling intraoral scanners may have their real data masked by this crucial factor. Conversely, others reinforce that the scanning pattern for digital acquisition does not significantly influence the clinical results obtained²³.

These studies were important to confirm the growing tendency to rehabilitate patients with the digital workflow. Nevertheless, even with scientific evidence, the number of dentists who have an intraoral scanner available is small, so to facilitate the choice of clinicians who have no experience with intraoral scanners, the best indication is the use of conventional molding with an open tray with splinting transfers^{1,10,12,17,24,25} and addition silicone as molding material¹³, which even promotes greater adaptation of the milled protocol bars, as shown by the results of this study.

The accuracy of scanning electron microscopy was used for image acquisition⁹ and later, the images were quantitatively evaluated for marginal fit. In addition to proving that the adaptation of the protocol bars of group A (digital models obtained by conventional molding followed by benchtop scanning) was superior to that of group B, in this group (intraoral scanner) overcontour and undercontour areas were observed in the distal and mesial regions. Although these misadaptations are observed, there are no statistical differences among the regions of group B (distal, central, and mesial). There were, however, differences among the regions evaluated in group A (central region with higher misadaptation than the mesial region). Even though this statistical difference was found, the primary outcome of the research was always the comparison among the groups. And in this context, regardless of the region, group A (conventional) always showed better adaptation than group B (digital).

Although the results of this study are important to guide the clinician's selection of the best technique for making the protocol bars, the acceptance, comfort, and time generated by the techniques must be considered during rehabilitation. Although the digital technique (B - intraoral scanner) has shown greater misadaptation than the conventional technique (group A), intraoral scanning is a well-accepted technique due to the comfort and agility in obtaining the images²⁶. Besides, another advantage of digital workflow is the ability to produce three-dimensional (3D) meshes to generate a virtual patient, enhancing the virtual treatment planning, communication with patients²⁷, and predictability^{26,28}. Considering that both methods promoted gaps that could generate biofilm accumulation and microleakage, and that

the patient must maintain adequate control of oral hygiene, the use of intraoral scanner cannot be ruled out.

For CAD-CAM crowns and short-span fixed partial dentures, intraoral scanning has been shown to be more accurate than conventional impressions²⁹⁻³¹. These studies describe marginal gaps of approximately 60 μm for CAD-CAM dental crowns produced by intraoral scanning, while conventional impressions exhibited gap values up to 183 μm ²⁹. In the present study, digital models obtained by conventional molding followed by benchtop scanning (group A) exhibited an overall marginal gap of 21.6 μm while the intraoral scanning produced an overall marginal gap of 39.2 μm , both significantly lower than those reported in the literature. The mean gap values differences among the studies are closely related to the type of rehabilitation, as it has been reported that the accuracy of intraoral scans is still challenging for extended rehabilitations³². Besides, authors have reported the differences among the software programs and methods for use in the digital design of dental prosthesis^{33,34}, and the influence of the operator's clinical experience and educational background. It has also been described that prosthodontists with basic CAD training were shown to outperform dental professionals who had CAD certificates but less clinical experience³⁴. Therefore, one important limitation of this investigation is that the interpretation of results should be performed carefully, as the materials and methods vary considerably among the studies. According to Cortes 2022³⁵, the outcomes of CAD-CAM restorations and prostheses can be affected during image acquisition (intraoral scan device, operator, technique, or anatomy), CAD phases (software or operator), or CAM phases (device, manufacturing material, CAM protocol, or finishing)³⁵.

In conclusion, and considering the described limitations, this study corroborates previous findings that the conventional molding technique followed by benchtop scanning presented better marginal adaptation than the digital technique performed with an intraoral scanner. However, future studies should compare different software programs, devices, and operation modes, and clinical studies must be performed to validate the obtained results.

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Conflict of interest

The authors have no conflicts of interest to declare.

Data availability

Datasets related to this article will be available upon request to the corresponding author.

Author contribution

- Renês Augusto Parizotto; methodology, investigation, data curation, writing (original draft, review, and editing).

- Vanessa Cavalli: methodology, formal analysis, data curation, writing (review and editing).
- Rafael Lacerda Zandoná: conceptualization, writing (review and editing)
- Geraldo Alberto Pinheiro de Carvalho: conceptualization, writing (review and editing)
- Aline Batista Gonçalves Franco: conceptualization, writing (review)
- Elimario Venturin Ramos: conceptualization, writing (review and editing)
- Sérgio Candido Dias: conceptualization, writing (review).

All authors actively participated in discussing the manuscript's findings and have revised and approved the final version of the manuscript.

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