

Development of Novel As-Cast Ti-Mo-Zr Alloys for Biomedical Applications

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Received: September 28, 2021; Accepted: October 20, 2021.

Titanium is one of the most utilized metals for orthopedic implants. This element has excellent mechanical and biological properties. As a strategy to develop a new system of alloys that do not cause health problems to the patient, such as the Ti-6Al-4V alloy, a new group of alloys has been designed to meet these expectations. Molybdenum, when associated with titanium, reduces the transition temperature from α to the β phase. Zirconium increases the corrosion resistance, decreases the melting point, and improves the alloy's biocompatibility. The alloys with the beta phase's predominance are the most desirable for biomedical applications due to their higher mechanical compatibility with the bone tissue. This paper presents the preparation of as-cast Ti-10Mo-xZr ($x= 30, 40,$ and 50 wt%) alloys and their characterization by measurements of density, energy dispersive spectrometry (EDS), x-ray diffraction, optical and scanning electron microscope (SEM). The density values were higher than that of pure titanium due to the zirconium and molybdenum. The EDS measurements reveal a suitable stoichiometry of the elements and no impurities contamination. In the x-ray diffraction and microscopy measurements, it was observed only peaks of the beta phase. This new system of Ti-alloys is promising for biomedical applications.

Keywords: *Ti-Alloys, β -phase alloys, Microstructure.*

1. Introduction

Titanium alloys have a high range of mechanical, physical, and corrosion resistance properties, which arouse an extreme interest in the aerospace, energetic, chemical, and health industries¹. Those alloys have some attributes and properties, either with high hardness, low elasticity modulus, or high melting point. Biomaterials play an important role in human development today. They can be divided into four major classes: metals and their alloys, polymers, ceramics, and natural materials².

Concerning health applications, the first alloys used were α -type alloys, such as commercially pure titanium and alloys developed for the aeronautical industry³. Then, the $\alpha + \beta$ type alloys gained attention, due to their wide range of properties, with the Ti-6Al-4V alloy being widely used today^{4,5}. However, there have been reports that aluminum and vanadium ions released into the bloodstream could cause cytotoxic effects and neurological problems (such as Alzheimer's disease)^{6,7}. This new class of titanium alloys has been looking for β -type alloys, as they have lower elasticity modulus, among all classes of titanium alloys^{8,9}. Such alloys have been produced with the addition mainly of molybdenum^{10,11}, zirconium¹²⁻¹⁵, tantalum^{16,17}, and niobium¹⁸⁻²¹, which are elements that do not present cytotoxic reactions with the organism.

The β metastable alloys consist of the predominance of the β -phase. However, it is still possible to contain small

fractions of the ω phase due to the thermomechanical processes derived from the production of this material. These alloys are used in structural applications where high strain resistance, stiffness, corrosion resistance, and low modulus of elasticity are required. These characteristics transform the metastable β alloys attractive to engineering and medicine, even considering their high production cost, as these materials also present excellent biocompatibility for the use of implants and interactions with bone tissue²².

Titanium in its entirety manages to change its crystalline structure in some temperature fields. Allotropic transformation is called a complete transformation from one crystalline structure to another, and when this phenomenon occurs, its transformation temperature is called the transition temperature²³. Pure titanium has a compact α -phase hexagonal structure at low temperatures. For values higher than the 882°C transition temperature, this assumes a cubic body structure centered with phase β ²⁴. Earlier studies state that the elasticity modulus for β -phase alloys is less than alpha-phase alloys¹. Molybdenum is a strong β -stabilizer and can have a wide range of compositions where the α and β phases of titanium can be present²⁵. The Ti-Mo system is a set of alloys widely studied because of their excellent mechanical properties, corrosion resistance, and low modulus of elasticity^{10,26-28}. Thus, for the alloy to present and stabilize characteristics referring to the beta phase, a minimum of 10% by weight of molybdenum is necessary^{28,29}.

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Zirconium is an element that belongs to the same group as titanium in the periodic table, presenting similar chemical properties³⁰. Zirconium acts as a strong hardening agent for the solid solution³¹. This element is easy to form solid solutions with titanium, which is added to improve mechanical and corrosion resistance and improve biocompatibility³². Adding zirconium can also decrease the martensitic transformation temperature (M_s) of the α' phase and slightly decrease the alloy's melting temperature^{14,15}. The Ti-Zr system has advantageous characteristics concerning its mechanical and biological properties, such as a higher tensile strength than commercially pure titanium, good biocompatibility, and higher elastic recovery. This factor provides this system high demand for dental applications³³.

In this context, this paper's purpose was to prepare and characterize a novel set of titanium alloys containing molybdenum and zirconium, aiming at biomedical applications. The alloys were obtained by arc-melting and characterized chemical, structural, and microstructurally to better understand this beta-type alloy's properties.

2. Materials and Methods

The alloys were prepared using the precursor elements of high purity, such as titanium (grade 2) in bars, zirconium in wire (98.5% purity), and molybdenum in wire (99.0% purity) in their proper proportions. The precursors were melted in an arc-fusion furnace, with a controlled argon atmosphere to prevent contamination, in a water-cooled copper crucible and the non-consumable tungsten electrode. The ingots were re-melted five times to ensure homogeneity. The ingots were cooled naturally into the furnace.

A chemical semi-quantitative microanalysis was performed using dispersive energy spectroscopy (EDS) in

an OXFORD detector, model INCA X-Act, coupled to the scanning electron microscope EVO LS15 by Carl Zeiss. Alloy elements were mapped to assess the material's distribution and homogeneity.

The density of the alloys was obtained by Archimedes principle, using an Explorer model Ohaus analytical balance.

The alloys' structure was obtained by X-ray diffraction measurements performed on a Rigaku diffractometer model D / Max 2100 / PC, with Cu-K α ($\lambda = 1.5406 \text{ \AA}$) radiation. The data will be collected using the powder method and fixed time mode, with a step of 0.02° ranging from 10° to 100° , and a collection time of 3.2 s.

Microstructural characterization was performed using an optical microscope Olympus BX51M model. Scanning electron microscopy images were obtained using an electron microscope Carl Zeiss EVO LS15 model. These microscopic techniques were used to observe the current phases and their distributions, the structure's quality, and the grains' size.

3. Results and Discussion

Figure 1 shows the energy peaks related to the composition of the alloy using the EDS technique. Through this technique, it was possible to obtain the chemical microanalysis of the produced alloys. Analyzing Figure 1 shows that it is possible to identify energy peaks related to the elements that compose the alloy: titanium, molybdenum, and zirconium. Table 1 shows the quantitative chemical analysis of the produced alloy using EDS. The data contained in Table 1 indicate a good melting of the system, where there is only a slight deviation concerning the composition of the alloys respecting the proposed stoichiometry. The ASTM F2066-13 standard³⁴ (which standardizes the Ti-15Mo alloy) states that the concentration of the elements must be $\pm 1 \text{ wt\%}$

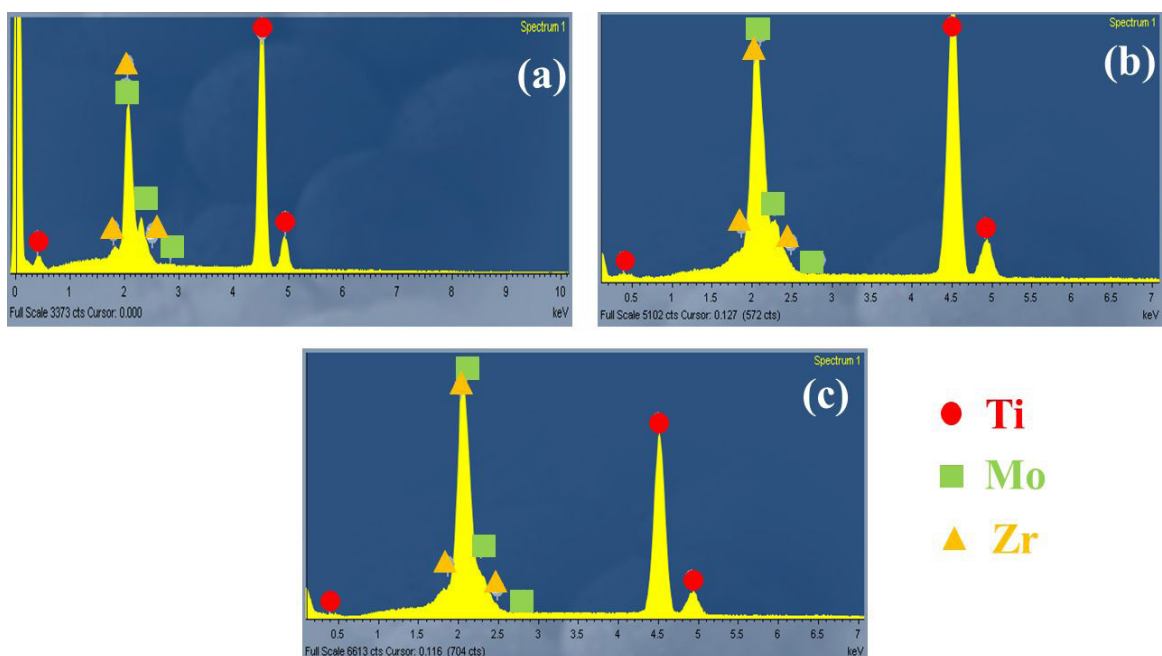


Figure 1. EDS spectra for Ti-10Mo-30Zr (a), Ti-10Mo-40Zr (b) and Ti-10Mo-50Zr (c) alloys.

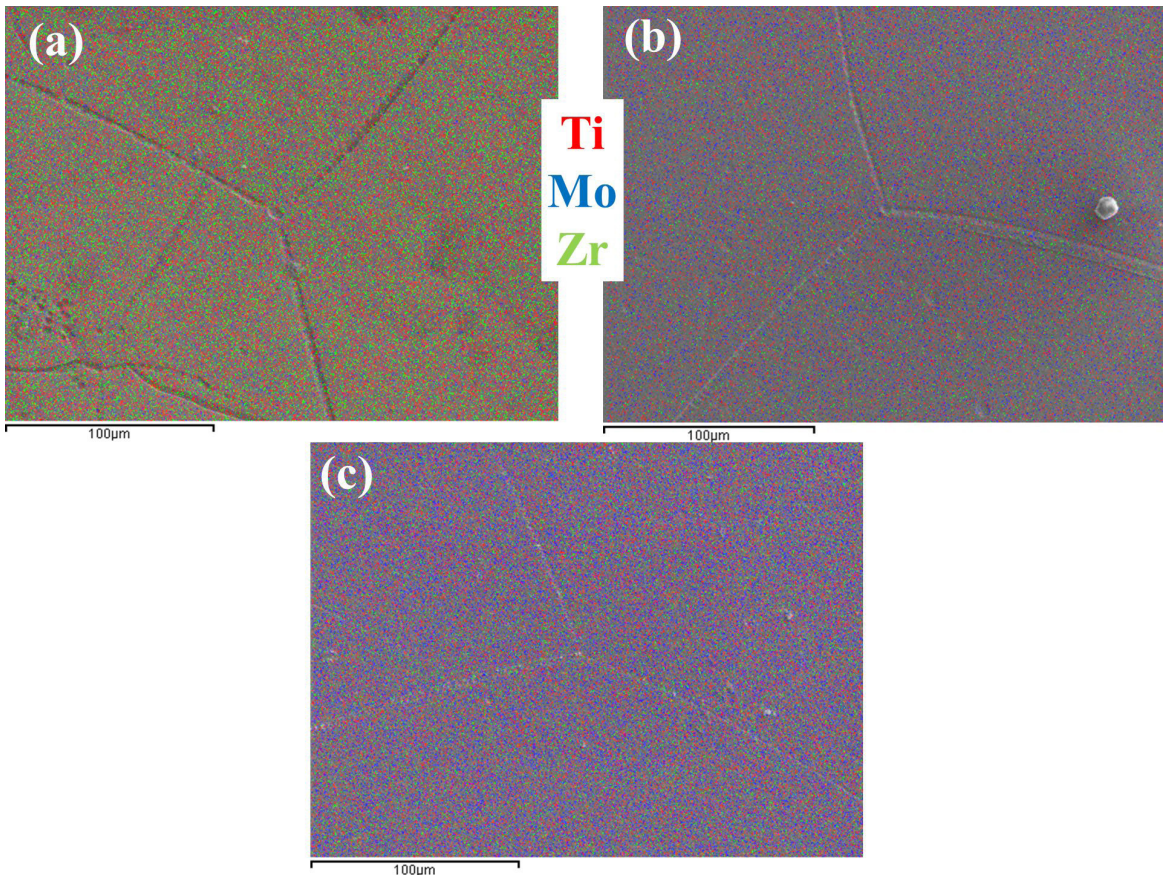


Figure 2. EDS elements mapping of the Ti-10Mo-30Zr (a), Ti-10Mo-40Zr (b), and Ti-10Mo-50Zr (c) alloys.

Table 1. Chemical composition of the Ti-10Mo-Zr produced alloys, obtained by EDS.

Element (wt%)	Ti-10Mo-30Zr	Ti-10Mo-40Zr	Ti-10Mo-50Zr
Mo	9.20	9.95	9.57
Zr	30.5	39.11	49.28
Ti	Balance	Balance	Balance

of the nominal concentration. The alloys of this study are within the established interval, validating the results of the chemical analysis.

In Figure 2, it can be shown the mapping of the compositions made by EDS, in which the red, blue, and green colors represent titanium, molybdenum, and zirconium, respectively. A good distribution of the elements, without precipitates or aggregates, was observed in all samples, indicating good homogeneity.

Regarding density, experimentally and theoretically obtained data are presented in Figure 3. Density is one of the important physical properties to study in biomedical materials, as specific strength is one of the criteria for biocompatibility³⁵. In the medical industry, low-density values are better, as they reduce the extra weight load on the organs around the implant, avoiding material stress³⁶.

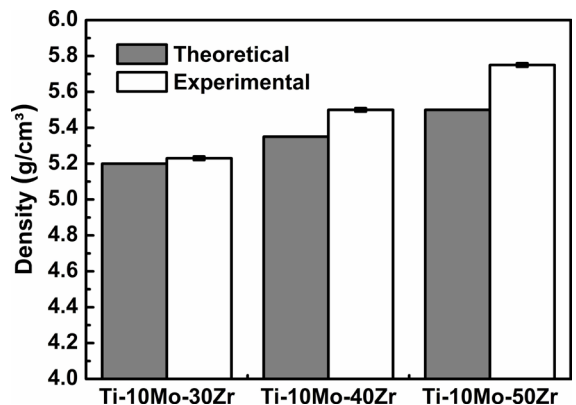


Figure 3. Density of the produced Ti-10Mo-Zr alloys.

The alloys in the Ti-Mo-Zr system stand out from the Ti-6Al-V (4.41 g/cm³), Cp-Ti (4.54 g/cm³), and Ti-15Mo (5.01 g/cm³) because they have high-density values. This fact is due to the addition of the elements Zr (6.51 g/cm³) and Mo (10.22 g/cm³) because, when added as alloying elements, they increase their density³⁷. Even with high values, the densities of the alloys presented in this paper are lower when compared to others used in the orthopedics field, such as stainless steel (7.5 g/cm³ and cobalt-based alloys (8,3 g/cm³)^{13,36}. When the

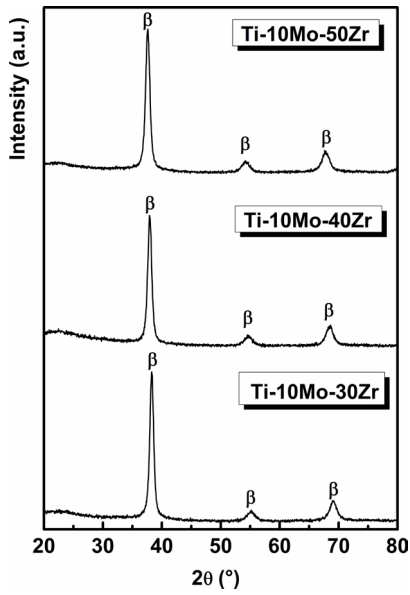


Figure 4. X-ray diffractograms for samples of as-cast Ti-10Mo-Zr alloys.

theoretical value is compared with the experimental value, an increase can be seen, which can be attributed to metallic impurities (Al, Cr, Fe, Mn, and Ni) and also to interstitial elements (O, C N, and H)³⁸.

Figure 4 shows the spectra obtained by X-ray diffraction for Ti-10Mo-30Zr, Ti-10Mo-40Zr, and Ti-10Mo-50Zr alloys. It can be observed only peaks related to the β phase. Ho et al.²⁸ studied Ti-Mo alloys and observed the beta stabilizing effect of molybdenum above 10% in weight as an alloying element. Zirconium is a neutral element, but when added as an alloying element together with another or more beta stabilizing elements, it can act as a beta stabilizing agent and help, therefore, in the consolidation of this phase¹³.

Figure 5 shows the micrographs obtained by optical and scanning electron microscope for the Ti-10Mo-Zr alloys.

According to Ho et al.³⁹, a characteristic morphological predominance of the β phase is observed by analyzing the obtained micrographs. These authors verified that with almost 10 wt% of molybdenum, only the beta phase's presence occurs. On the other hand, zirconium acted as a neutral element, maintaining the beta phase without other phases during the analysis as the proportions increased.

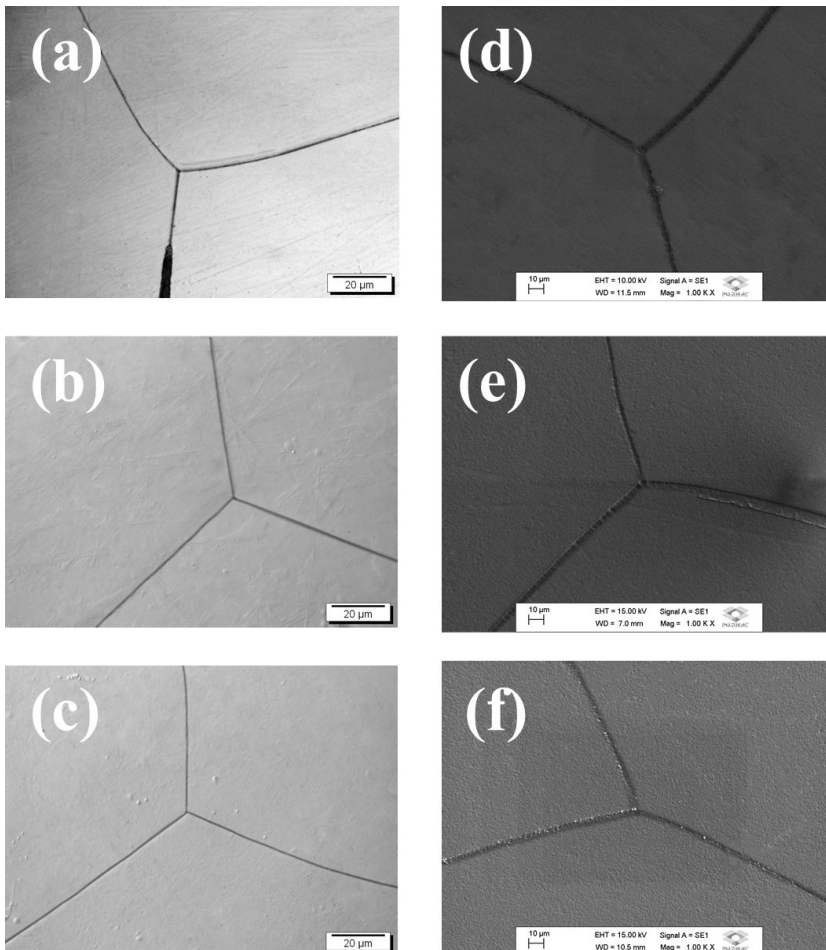


Figure 5. Optical micrographs for Ti-10Mo-30Zr (a), Ti-10Mo-40Zr (b) and Ti-10Mo-50Zr (c) alloys; scanning electron micrographs Ti-10Mo-30Zr (d), Ti-10Mo-40Zr (e) and Ti-10Mo-50Zr (f) alloys.

4. Conclusions

From the obtained results, it is possible to conclude that the as-cast Ti-10Mo-Zr alloys have an intense beta phase by the X-ray diffraction and microscopy measurements. These preliminary results make it possible to conclude that the produced alloys can be applied as a biomaterial, completing the study with some mechanical tests (as hardness and elasticity modulus) and biocompatibility tests.

5. Acknowledgments

The authors would like to thank Professor Oscar Balancin and Rover Belo (UFSCar) for using hot-rolling equipment. This study was financed in part by the Coordenação de Aperfeiçoamento de Pessoal de Nível Superior - Brasil (CAPES) - Finance Code 001 and CNPq (grants #308.204/2017-4 and #148.171/2019-2).

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